



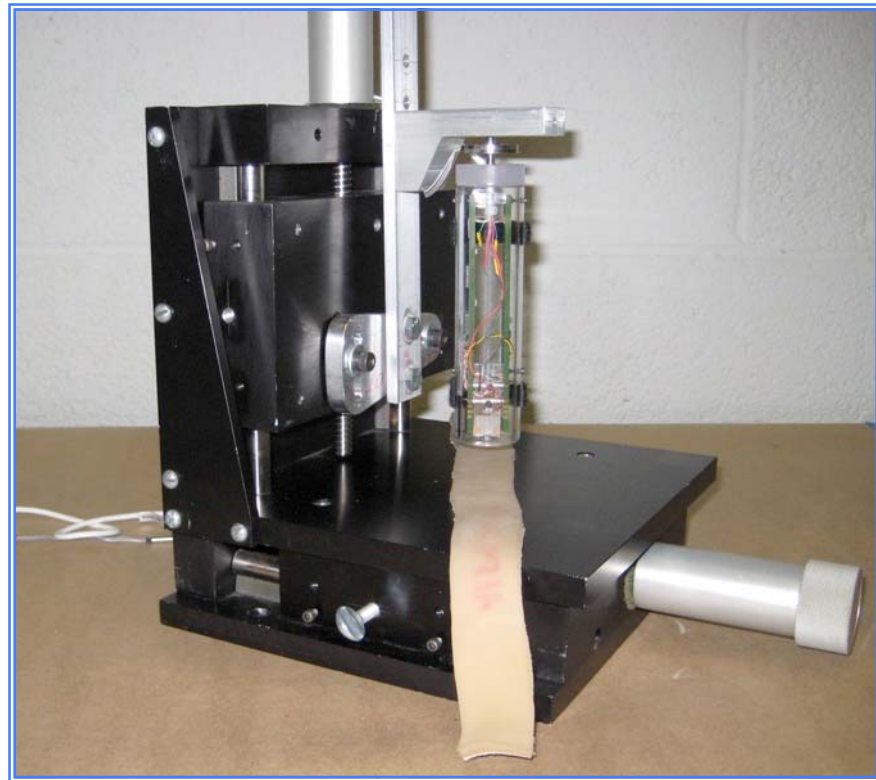
Testing the Skin Interrogation Device

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Research Project Presentation
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Outline

- Introduction
 - Significance
 - The Skin Interrogation Device
- Project Objectives
- Methods
- Results
- Conclusions



Introduction

My Purpose: perform bench tests to evaluate particular aspects of the prototype “skin interrogation device”

- Device developed by CATEA and McGill University
- *Device purpose*: in-vivo measurement of the skin’s mechanical properties.



Significance

- Detection of disease
- Evaluate effectiveness of therapeutic interventions
(Edwards & Marks 1995, Greenleaf et al. 2003)
- Guidance for orthotic and prosthetic device recommendations

(Mak et al. 1994)



(Clip Art)

Significance

- Predominant methods:

- ☐ Visual inspection
- ☐ Physical palpation



- Problems:

- ☐ Inherently subjective and may vary with clinician experience and skill

(Mak et al. 1994, Edwards & Marks 1995, Lee et al. 2007)

- More objective alternatives seem to have limited accessibility.

The Skin Interrogation Device

- Piezoelectric benders
- Strain gages

Design Objectives

- Quantify in-vivo mechanical properties of the skin
- Point-of-care technology
 - ☐ Low cost
 - ☐ Portable
 - ☐ Simple to use
 - ☐ Robust



Project Objectives

Reliability: Is the performance of the device affected by the following variables?

- 📁 Ambient temperature and humidity
- 📄 Normal force
- 📄 Angle of approach

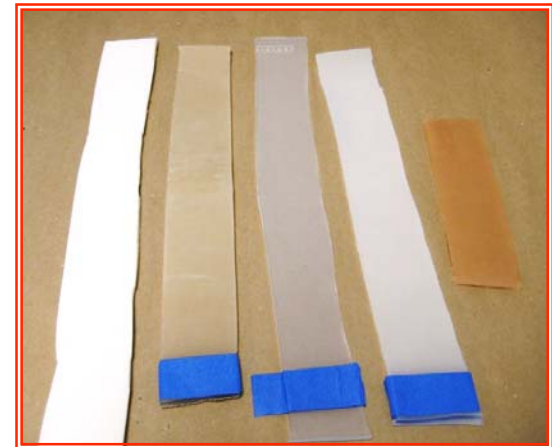
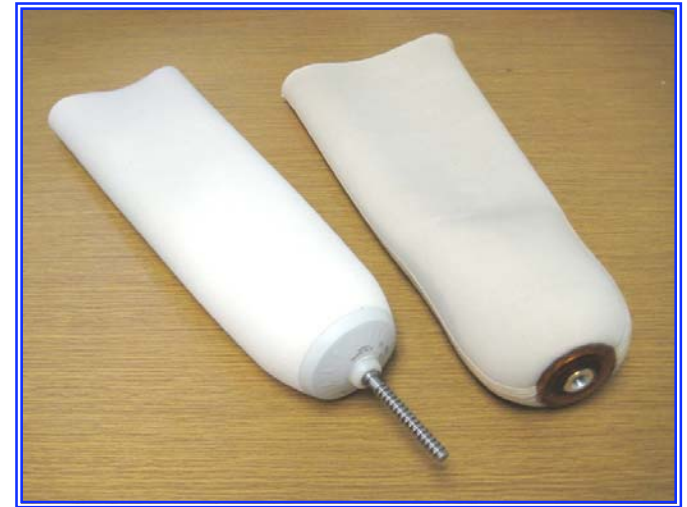
Validity:

- 📁 Able to differentiate materials with different properties?
- 📄 Define the relationship: device output to known properties



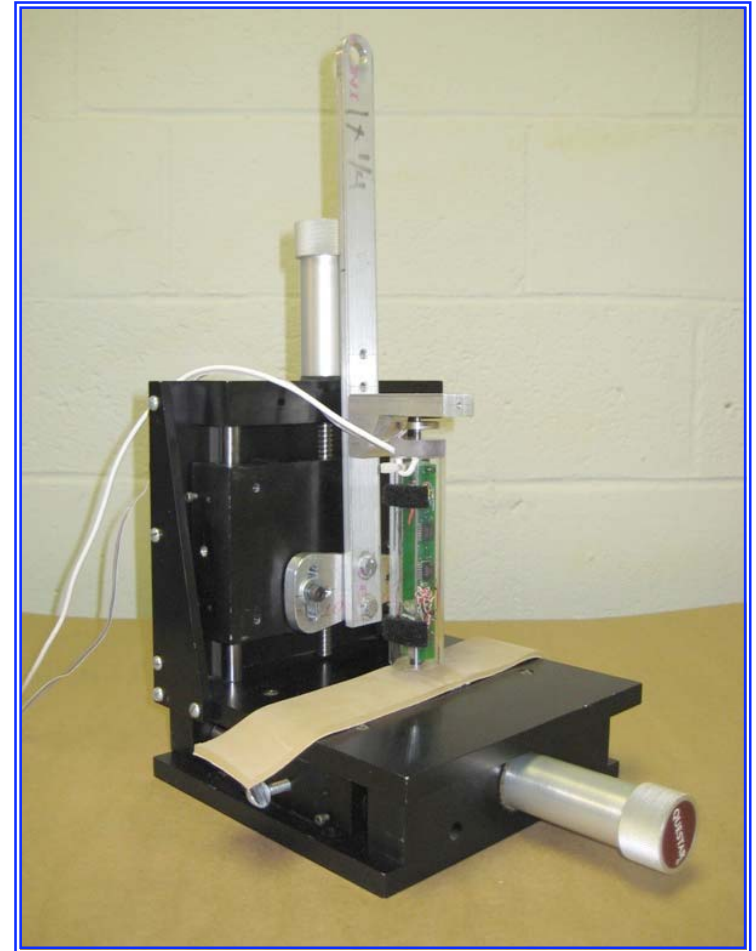
Methods: Materials

- Test material = commercially available prosthetic liners
- $n = 12$ different liners
- Properties known
(Sanders et al. 2004)
- Tested in Randomized order



Methods: Set-up

- Bench-top Positioning Device
- Load Cell
- Constant loading conditions
 - Application force = 5N
 - Approach angle = vertical
- 8 trial repetitions per liner





Data Analysis

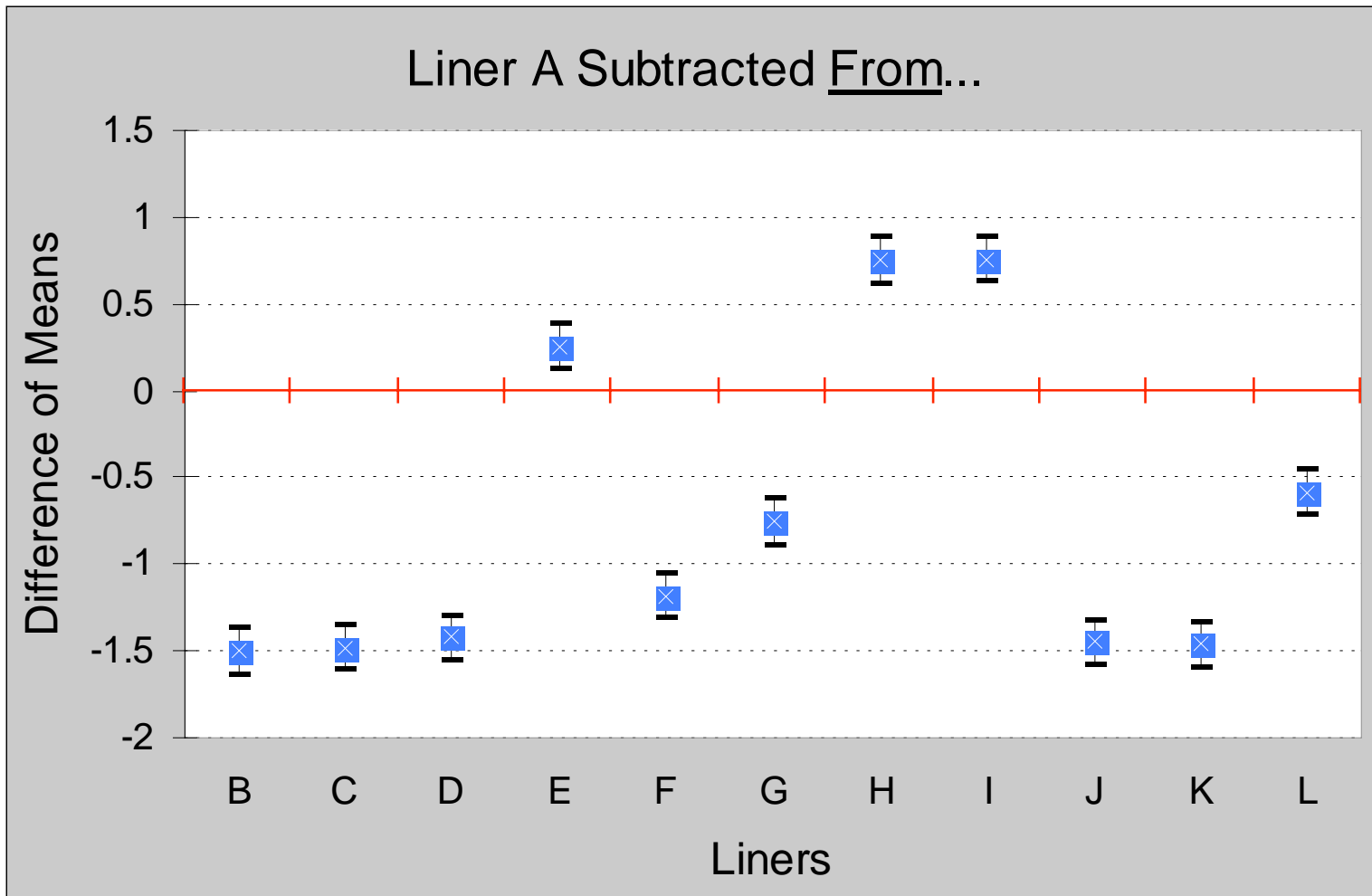
- Data Format = approximate stiffness based on strain gage voltage

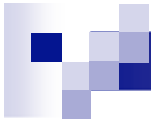
Statistics

- Liner Differentiation:
 - Un-paired ANOVA ($\alpha = 0.05$)
 - Tukey's post-hoc tests (confidence intervals = 95%)
- Relationship to known properties:
 - Regression Analysis
 - Response Variable = approximate stiffness from SID
 - Explanatory Variable = reported shear stiffness

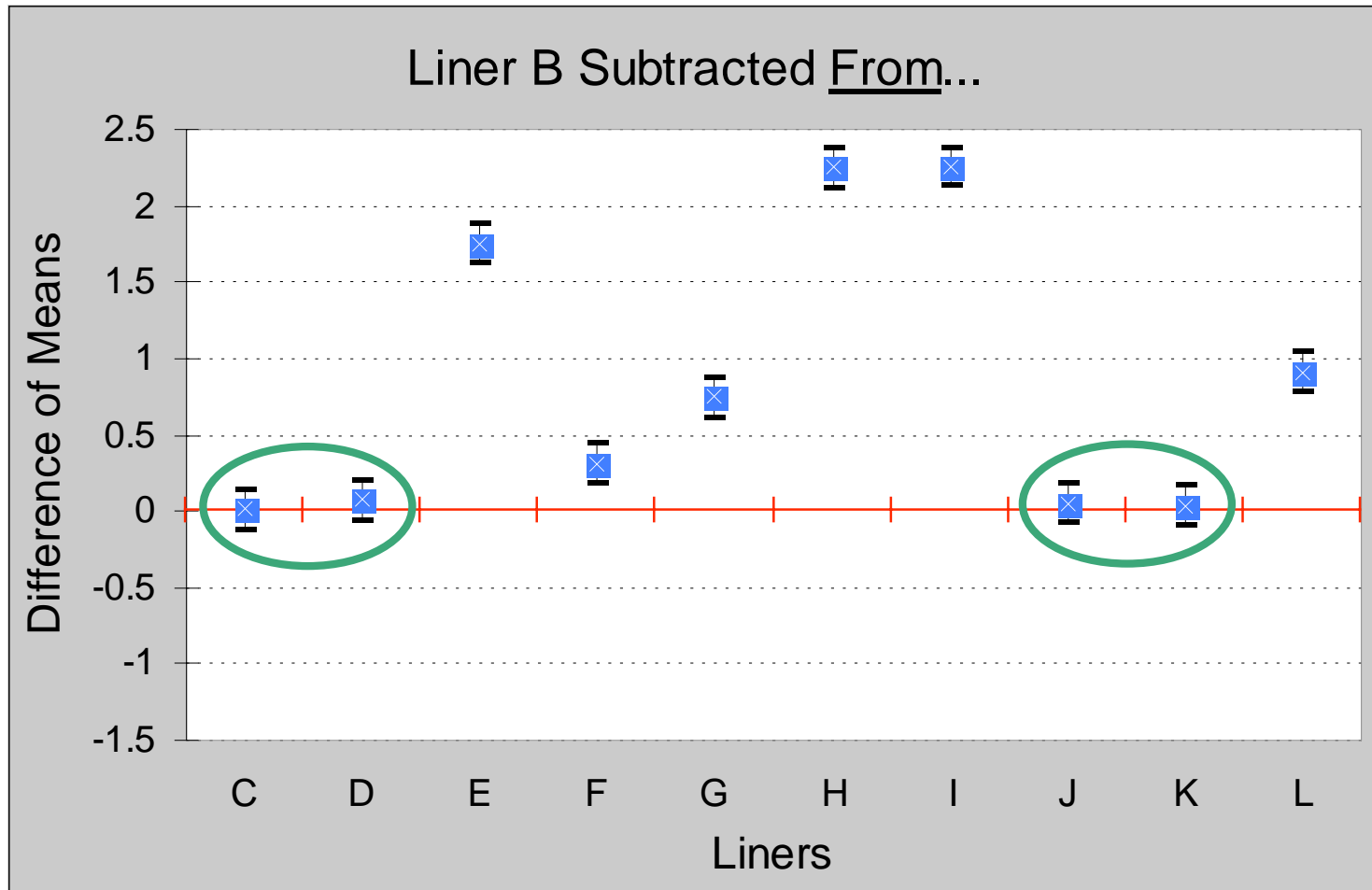
Results: Able to differentiate materials?

■ Example 1:





■ Example 2:



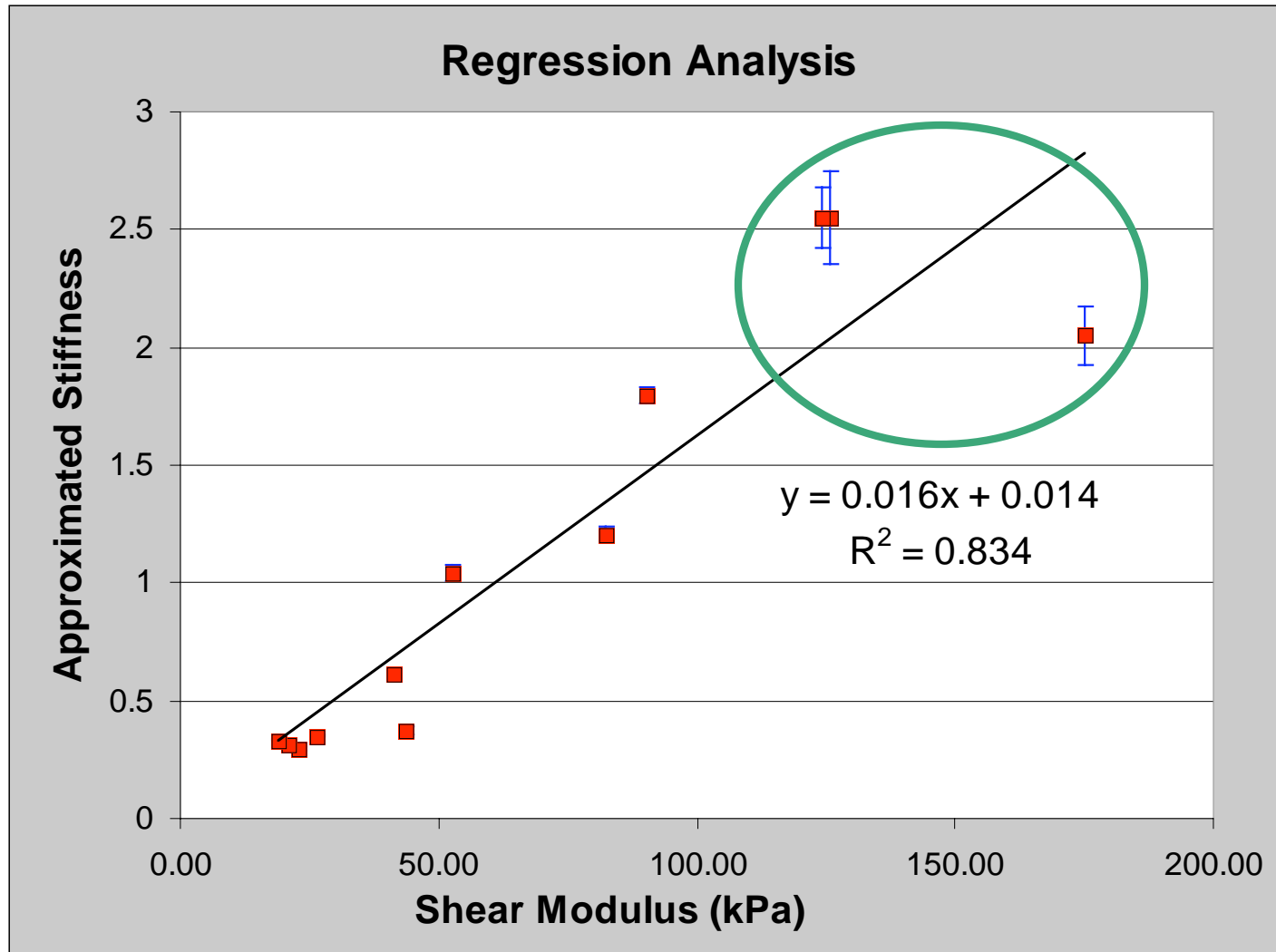
■ Overall: differentiated 55 of 66 (83%) liner pairs



Results: Able to differentiate materials?


Changing Variable	Mean % Difference
Temperature Range (69.4° to 75.2°)	2.21%
0.8N change in Application Force	13.58% (0.69 to 31.00)
4° variation in Approach Angle	30.52% (1.05 to 74.07)
Liner Comparisons	82.45% (0.13 to 158.76)
Pathology Example: Scleroderma	68% stiffer than unaffected skin (Edwards & Marks 1995)


Results: Relationship between device output and known properties?





Conclusions

 Changes in the prototype's output do appear to reflect changes in stiffness properties.

 The prototype is capable of differentiating materials that have differences in these stiffness properties.



Conclusions

■ Limitations:

- Unknown differences between my liners and those studied by Sanders et al. in 2004
- Prosthetic Liners \neq Skin

■ Future Work:

- Sensitivity analysis using physical models of skin morphology.
- Human subject trials to assess validity in the clinical setting.



References

- Edwards C, Marks R. Evaluation of biomechanical properties of human skin. *Clin Dermatol* 1995;13:375-380.
- Greenleaf JF, Fatemi M, Insana M. Selected methods for imaging elastic properties of biological tissues. *Annu Rev Biomed Eng* 2003;5:57-78.
- Lee BY, Butler G, Al-Waili N. Noninvasive assessment of visco-elasticity in the presence of accumulated soft tissue fluid. *J Surg Res* 2007;141:289-293.
- Mak AFT, Liu GHW, Lee SY. Biomechanical assessment of below-knee residual limb tissue. *J Rehab Res Dev* 1994;31:188-198.
- Sanders JE, Nicholson BS, Zachariah SG, Cassisi DV, Karchin A, Fergason JR. Testing of elastomeric liners used in limb prosthetics: classification of 15 products by mechanical performance. *J of Rehabil Res Dev* 2004;41(2):175-186.
- Wang Q, Hayward V. In vivo biomechanics of the fingerpad skin under local tangential traction. *J Biomech* 2007;40:851-860.
- Wang Q, Kong L, Sprigle S, Hayward V. Portable gage for pressure ulcer detection. Paper presented at the 28th IEEE EMBS Annual International Conference, New York, NY, August 30 – September 3, 2006.



Thank You

- CATEA

- ☐ Dr. Sprigle
- ☐ Jayme Caspall
- ☐ Ricardo Lopez
- ☐ Jonathan Jowers

- Prosthetic Liner Providers

- ☐ Ossur, OttoBock, OWW, Alps, Silipose, ESP



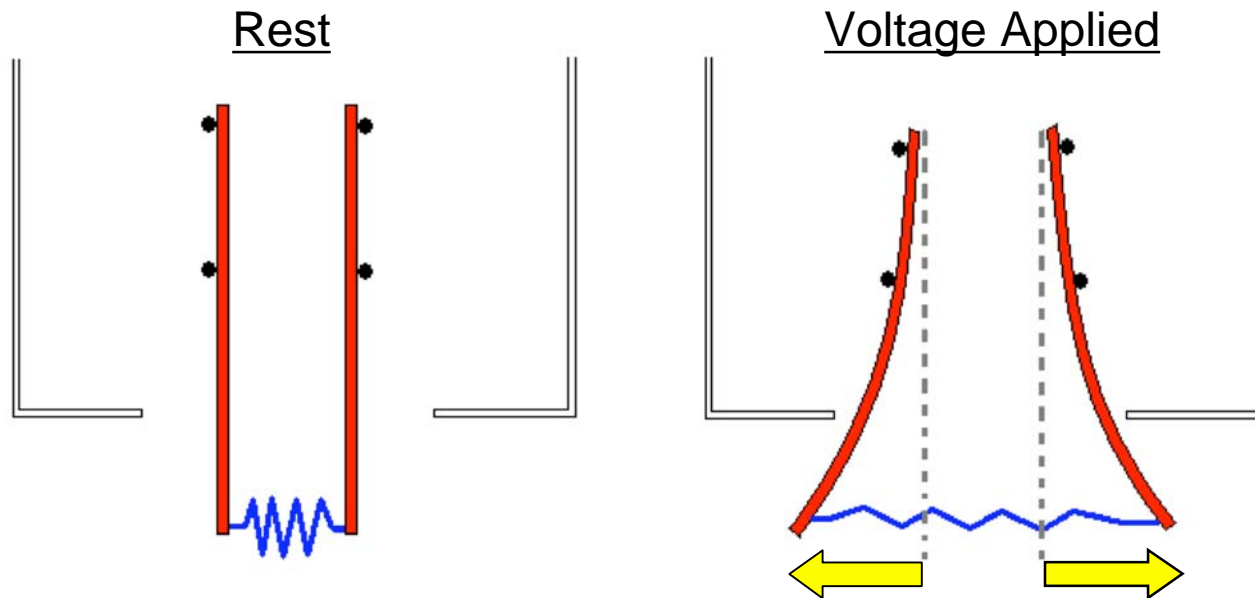
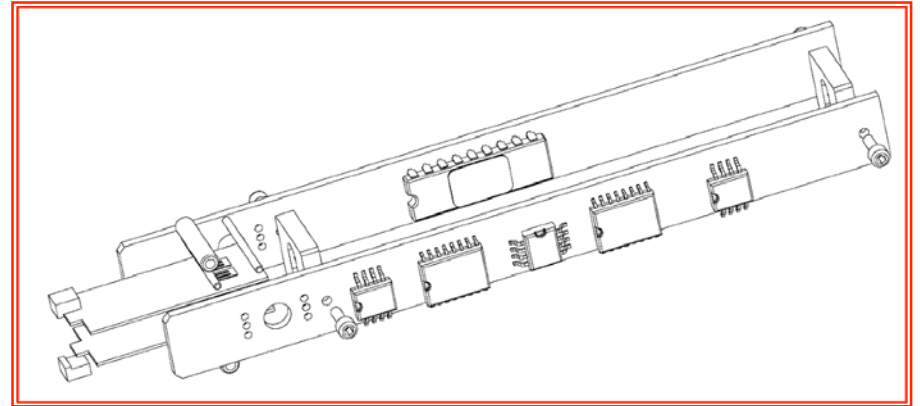
Questions?



Extra Slides

The Skin Interrogation Device

- Benders actuate to apply stress to isolated region of skin
- Strain Gages
- Load cell
- Feet with High Friction Coating
- LabView Software Interface

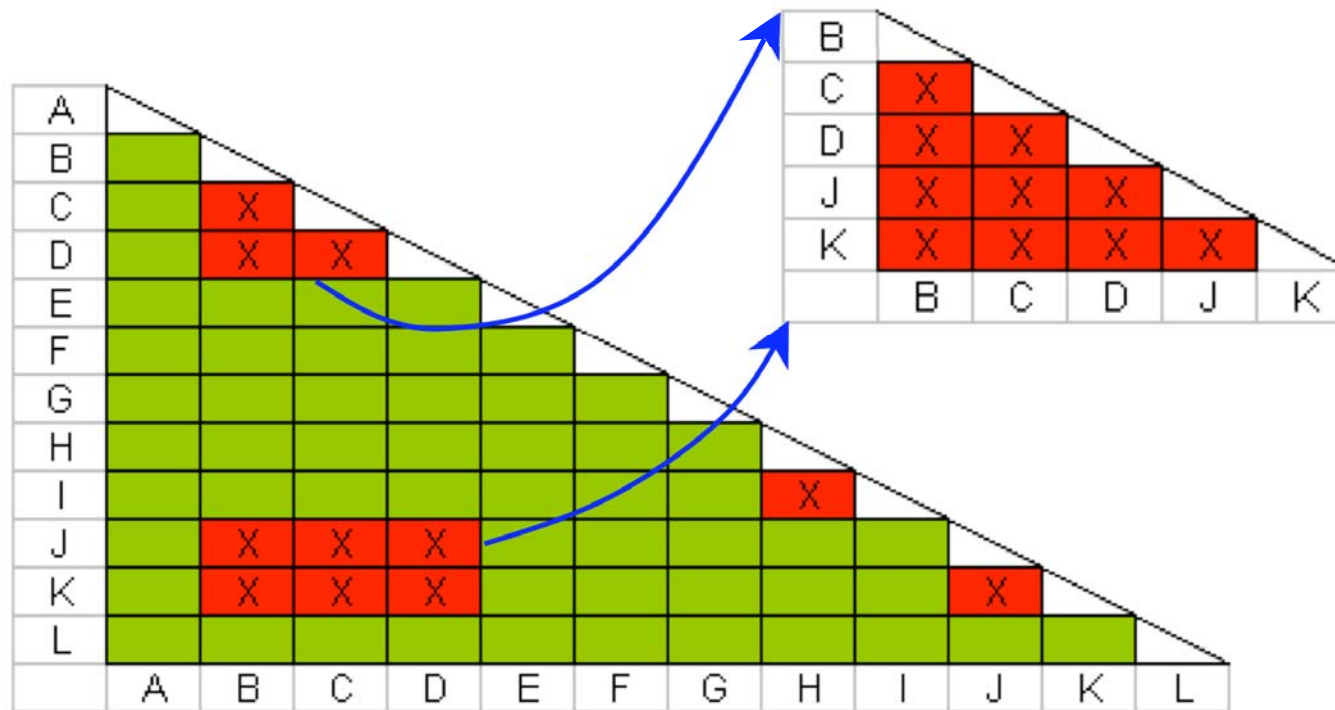


Liners

(Sanders et al. 2004)		Material Composition	Fabric Backing?	Sample Thickness (mm)	Sanders Thickness (mm)	Shear Modulus (kPa)	Approximate Stiffness	
Liner Pair							mean	st dev
Alps ELDT 6mm	B	silicone gel	yes	5.9	5.6	23.28	0.2929	0.0062
Alps Super Stretch	C	silicone gel	no	6.5	6.12	21.19	0.3074	0.0033
ESP Aegis Ultimate	D	silicone gel	yes	5.4	5.1	43.99	0.3703	0.0183
Alpha 9mm	J	silicone gel	yes	9.3	9.42	26.49	0.3449	0.0033
Siloliner	K	silicone gel	yes	5.1	5.21	19.29	0.3291	0.0076
Iceross Original 2-color	H	silicone elastomer	no	2.1	2.27	125.92	2.5449	0.1946
Iceross Original Clear	I	silicone elastomer	no	3.3	3.36	124.54	2.5481	0.1288
Alps Clearpro	A	silicon elastomer	no	3.2	2.06	90.54	1.7906	0.0324
ESP Streamline	E	silicone elastomer	no	2.0	2.19	175.2	2.0452	0.1244
Iceross Dermo 6mm	G	gel silicone	yes	6.1	5.81	52.86	1.0388	0.0355
Profile Urethane	L	urethane	no	6.8	6.29	82.73	1.2032	0.0312
Iceross Comfort Plus	F	silicone elastomer	yes	6.0	5.89	41.55	0.6084	0.0148

- Mak et al. 1994: soft tissue measurement on the lower limb yielded elastic modulus results 21 to 195 kPa.

More on Liner Differentiation



X p-value > 0.05
 p-value < 0.05

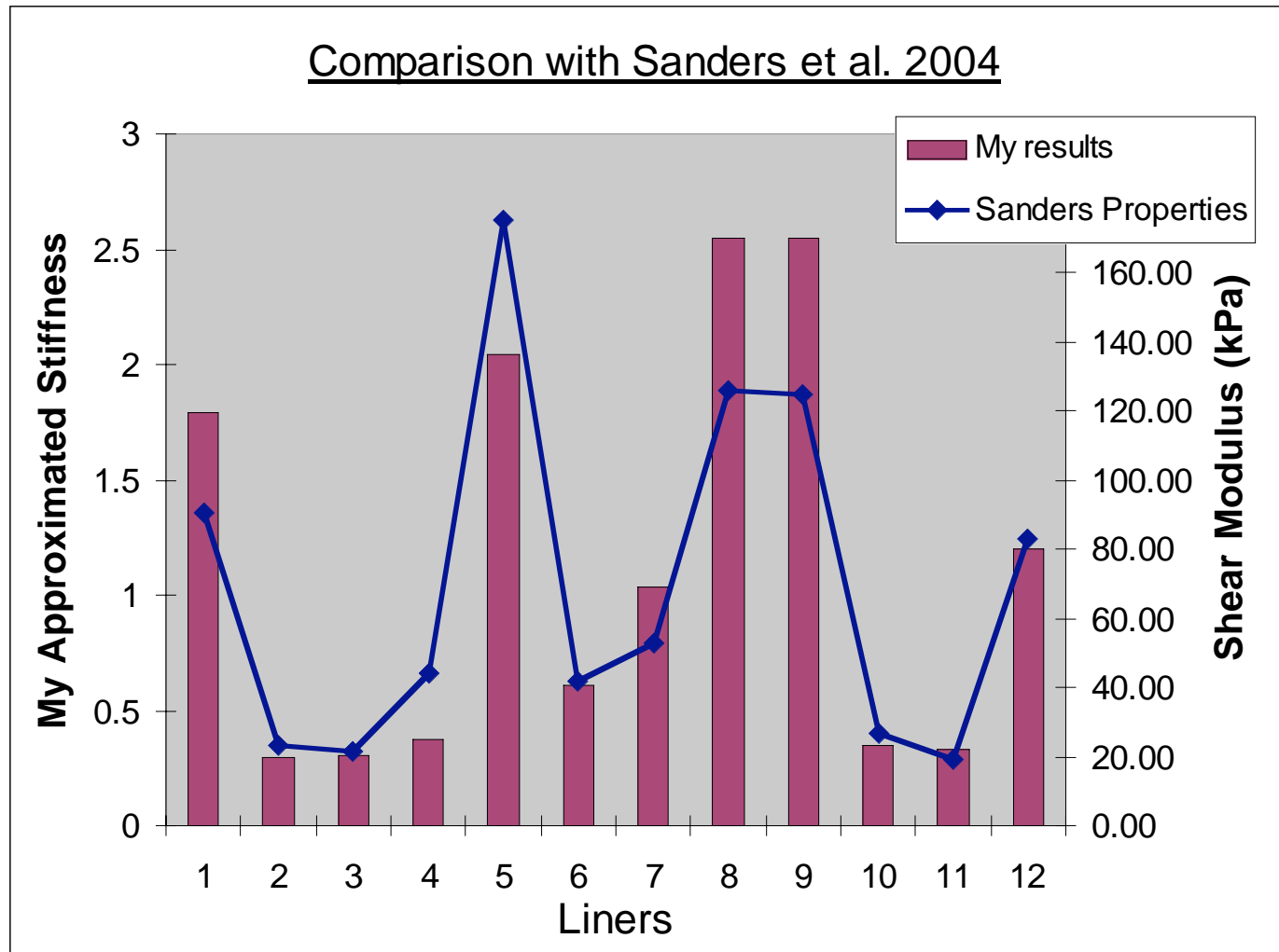
- Liners BCDJK are the only silicone gels
- Liners H & I: Sanders et al. report only 1% difference in shear modulus properties

Liner Limitation

New Liner	Older Liner	% Difference in Approximated Stiffness
ESP Aegis Ultimate (new)	ESP AEGIS Z (old)	3.14
Iceross Dermo 6mm (new cut)	Iceross Dermo 6mm (old)	31.79
Iceross Original Clear 2mm (new)	Iceross Original Clear 2mm (old)	17.47
TEC (OttoBock) Urethane (new)	TEC Urethane (old)	9.22



Results: Relationship between device output and known properties?



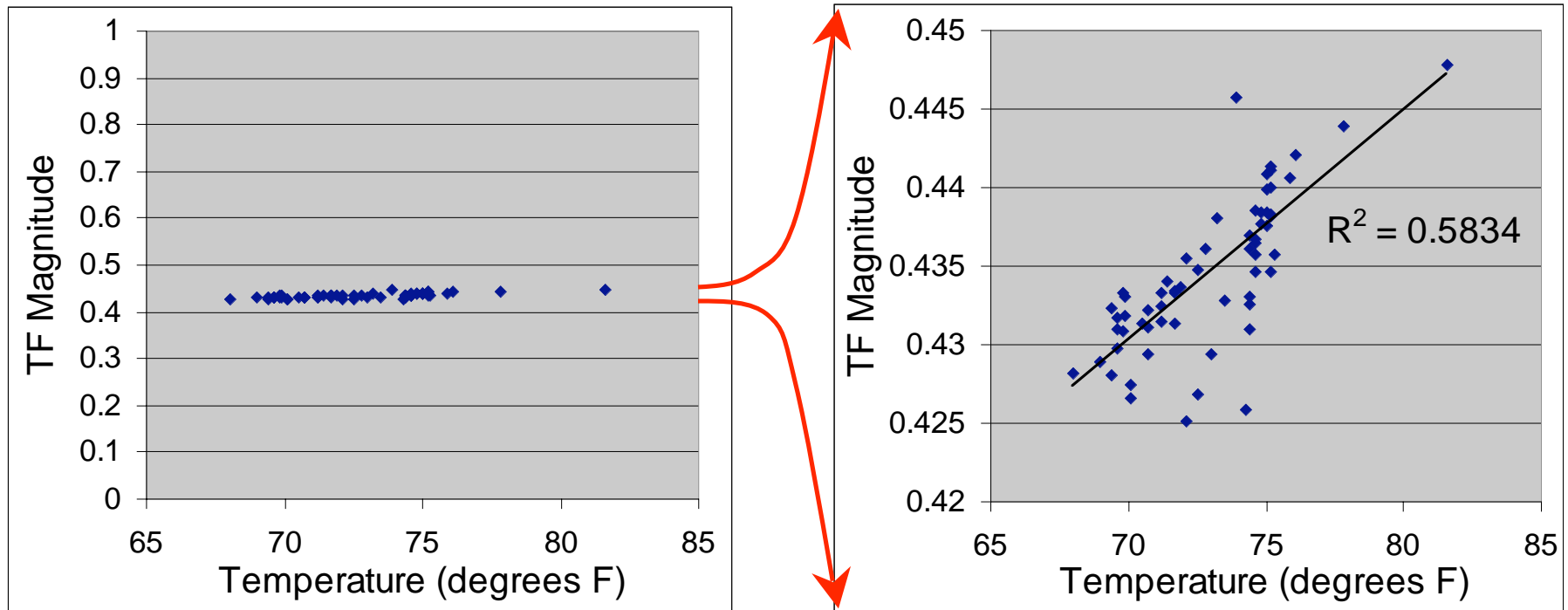
Methods: Ambient Conditions

- Unloaded tests
- Range of ambient temperature and humidity conditions
 - Not actively manipulated
 - **Temp**: 68°F to 81.6°F
 - **Humidity**: 25% to 72.5%



(EXTECH Instruments)

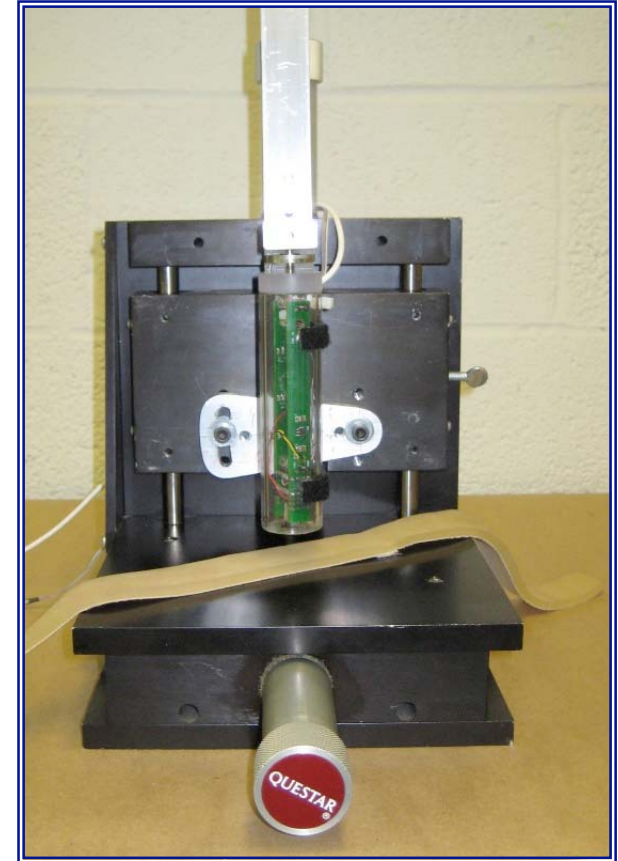
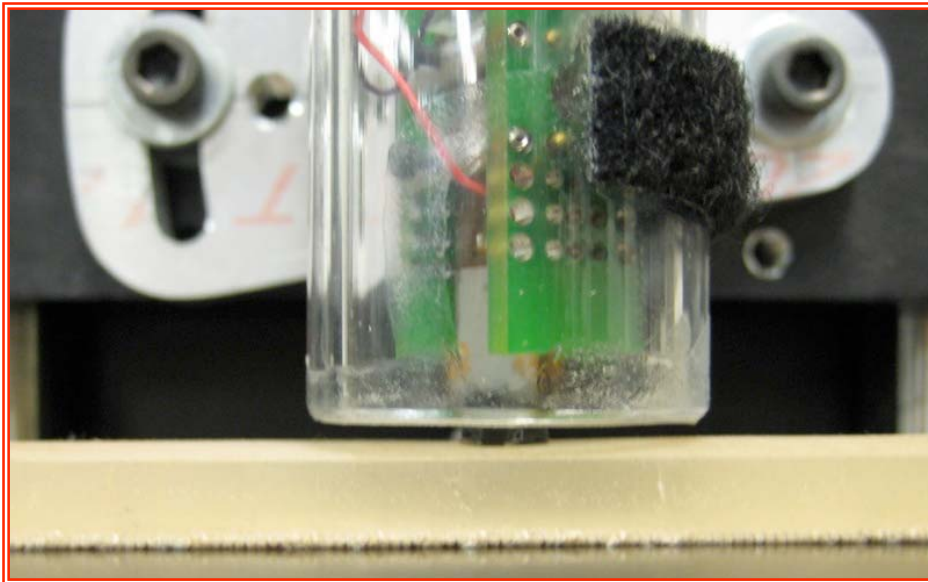
Results: Ambient Conditions



■ $CV = 1.2\%$

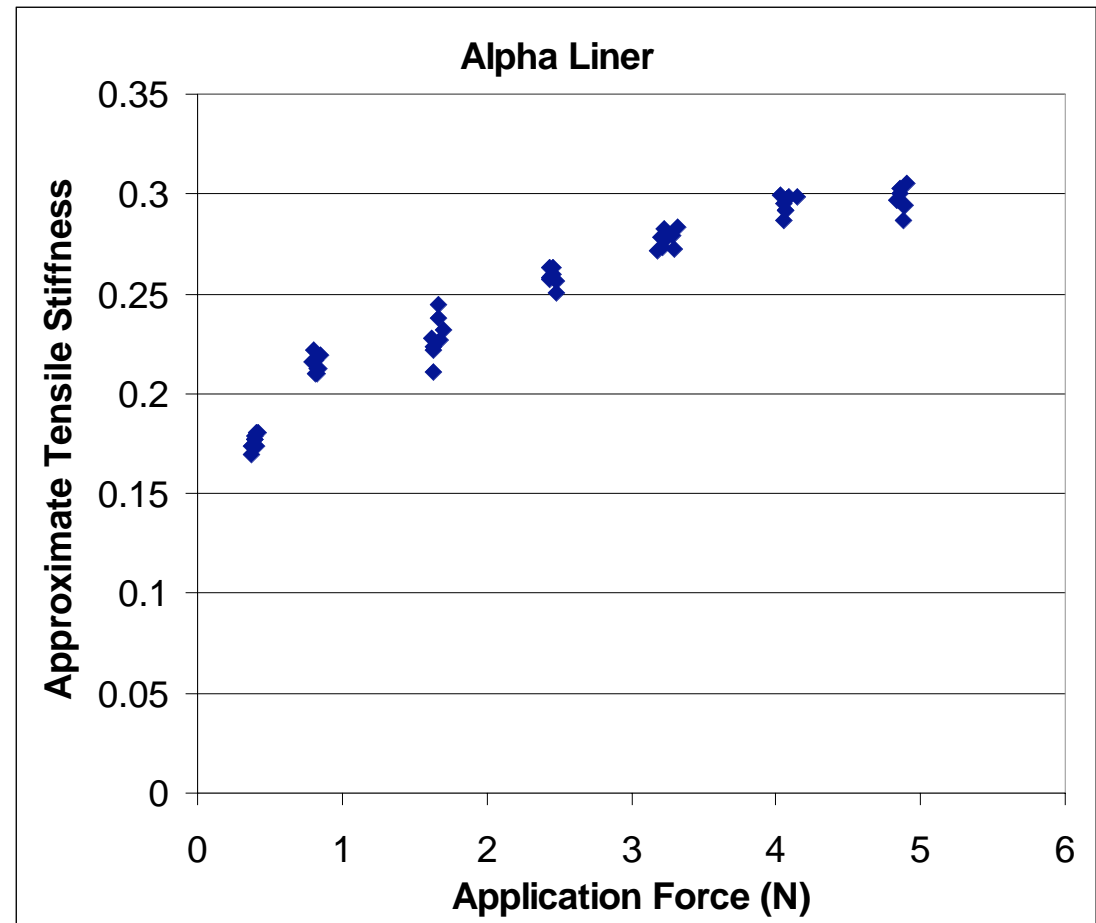
Methods: Application Force

- Loaded tests
- Range of application forces:
 - Eight levels between 0.0 to 5.0 N
- Effect of force compared for different material and frequency conditions
- 8 repetitions per combo of conditions



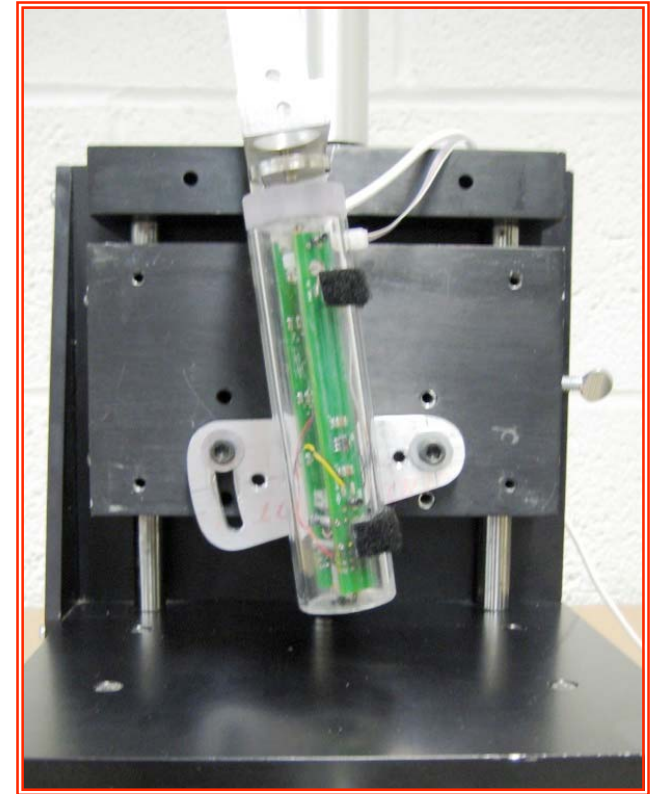
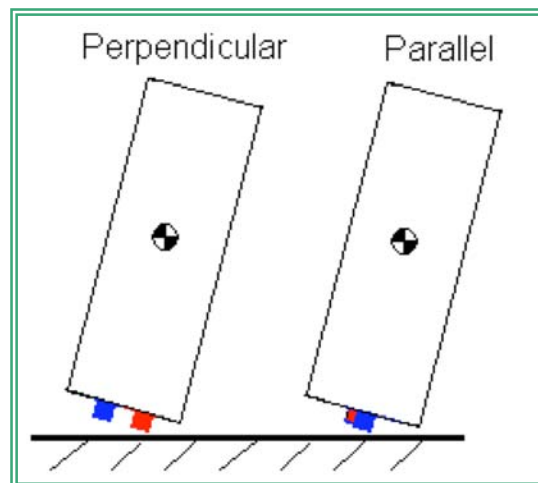
Results: Application Force

- Clear sensitivity to force of application
- **Conclusion:**
 - Usage protocol should include precise control of force



Methods: Approach Angle

- Loaded Tests
- Range of Angles: 0, 2, 4, 6, 8°
- 2 orientations:
 - Feet parallel to rotation axis
 - Feet perpendicular
- Effect of angle compared for different material and force conditions
- 8 repetitions per scenario



Results: Approach Angle

